

# Quality Assessment of Hyperpolarized <sup>129</sup>Xe Magnetic Resonance Image (MRI) **Data from Healthy and Asthmatic Patients With Varied Compressed Sampling** Mitra Tavakkoli<sup>1,2</sup>, Sarah Svenningsen<sup>2,3</sup>, Norman Konyer<sup>2</sup>, Parameswaran Nair<sup>3</sup>, Michael D. Noseworthy<sup>1,2,4,5</sup>

## Introduction

- Hyperpolarized (HP) <sup>129</sup>Xe MRI has shown great promise in capturing pulmonary disease information. Hyperpolarization enhances the NMR signal or MR image quality, and it can be divided into two steps: 1) optical pumping and 2) spin exchange. Figure 1 represents a simple schematic of these two steps for <sup>129</sup>Xe hyperpolarization [1]. In this technique, the signal comes from the nuclear magnetic moment of spins from <sup>129</sup>Xe instead of the hydrogen spins of water, as in conventional MRI. Figure 2 shows an example of HP <sup>129</sup>Xe lung MRI compared to conventional <sup>1</sup>H MRI. However, this approach requires breath holding during acquisition, which is problematic in asthma patients [2,3].
- Accelerated imaging methods such as Compressed Sensing (CS) allow good quality image recovery from undersampled MRI data permitting faster data acquisition [4]. CS is now becoming routine for <sup>1</sup>H MRI. However, its application in HP <sup>129</sup>Xe lung ventilation MRI has not yet been optimized. Thus, our aim was to assess CS sampling schemes and their effect on image quality (SNR and resolution).

Proton Lung MRI

HP <sup>129</sup>Xe Lung MRI



**Figure 2** Left) <sup>1</sup>H lung MRI Right) HP <sup>129</sup>Xe lung MRI

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**Figure 1** A simple representation of <sup>129</sup>Xe polarization [1]

### Methods

- Subjects: Inhaled HP <sup>129</sup>Xe datasets from 10 subjects (5 healthy and 5 asthmatic) were used
- Image Acquisition: Images were acquired on a 3.0 T MRI (Discovery MR750, GE, acquiring fully sampled 3D multi-slice HP-<sup>129</sup>Xe lung ventilation images (128x80, 16 slices) [5].
- Image Processing: 200 masks were pseudorandomly generated [6] each at 7 different sampling rates, (15% to 75% , step length =10%). The Parallel Imaging Compressed Sensing (PICS) command from the Bart toolbox [7], with L1 wavelet optimization and 100 iterations, was used to reconstruct undersampled data. Resultant image quality (SNR, incoherence value, resolution, statistical similarity (SSIM)) for each was compared (figure 3).

# Results

With greater undersampling, the degree of incoherence and SSIM decreased while the SNR increased. However, a high degree of variation in all quality metrics were noted for each of the undersampling rates. Relative Standard Deviation (RSD) values showed that SNR varied as much as 77.21% , SSIM 64.1%, and incoherence value 51.55%, depending on sampling scheme.

### Discussion

These results indicate there is an optimized rate **1.** Roos, Justus E., et al. (2015) *Magnetic Resonance Imaging Clinics* 23(2): 217-229. **2**. Hans-Ulrich K, et al. (2018) MRI of the Lung. and pattern of undersampling. This needs thorough Vol. 6. Springer International Publishing. 3. Roos JE, et al. (2015) Magn. investigation to determine optimal CS accelerated Reson. Imag. Clin. 23(2):217-229. 4. Lustig M, et al. (2008) IEEE signal processing magazine 25(2):72-82. 5. Svenningsen, Sarah, et al. (2021) HP 129Xe lung ventilation imaging and preserve Academic radiology 28(6):817-826. 6. Kojima S, et al. (2018) Radiol. fine image detail while reducing acquisition time. Phys. Tech. 11(3):303-319. 7. Uecker M, et al. (2013) ISMRM Workshop on Data Sampling and Image Reconstruction.



**Fully Sampled** 

Sampling Rate= 35%



Figure 3. Comparing varying levels of undersampling in both asthmatic (top) and healthy (bottom) resultant lung images. The SNR values varies from 25.17 to 89.25 in the asthma case, and 65.84 for the healthy patient (fully sampled image SNR: 25.17)

## References



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Aug 27th 2021

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